

Letter

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TiO2 Nanotube Arrays Modified Titanium: A Stable, Scalable, and Cost-Effective Bioanode for Microbial Fuel Cells

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2 Bioanode for Microbial Fuel Cells

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19 **TOC Art:**



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22 Abstract:

Titanium has been widely used as a dimensionally stable anode in the electrolysis 23 24 industry because of its excellent corrosion-resistance, conductivity, and scalability. 25 However, due to its poor biocompatibility and low performance as bioanode, it has 26 drawn little attention in the field of microbial fuel cells (MFCs). This study reports an 27 efficient way to convert titanium electrode into a high-performance anode for MFCs, 28 in-situ growth of titanium dioxide nanotubes (TNs) on its surface. After TNs 29 modification, the titanium surface became rougher, more hydrophilic, and more conducive for anodic biofilm formation. The maximum current density achieved on 30 this TNs-modified titanium electrode was 12.7 A m^{-2} , which was 190-fold higher than 31 32 the bare Titanium electrode and even higher the most-commonly used carbon felt electrode. Therefore, the high conductivity, corrosion-resistance, and current density 33 34 make TNs-modified titanium electrode a promising and scalable anode for MFCs.

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37 INTRODUCTION

Microbial fuel cell (MFC) is an emerging technology that can directly convert organic 38 waste into electrical energy through the metabolism of electrochemically active 39 microorganisms (EAMs).¹ In past decades, remarkable improvements have been 40 achieved in MFCs in terms of increasing power/current density, finding new electrode 41 42 materials, optimizing reactor configurations, and understanding EAMs. However, 43 scaling this technology for practical application is still limited by low power density 44 and high capital cost. The electrodes are the core components that determine the cost 45 and the performance of MFCs. Thus, finding cost-effective electrode materials has drawn increased recent attention and a variety of novel electrodes have been 46 reported.² 47

Due to their excellent biocompatibility and chemical stability, carbon-based 48 49 electrodes in various configurations (e.g. paper, cloth, felt, foam, brush) have been extensively used in MFCs.³ However, their low electrical conductivity and mechanical 50 51 strength remain major obstacles for their practical application at larger scale. Consequently, metal-based electrodes, such as gold, silver, copper, nickel, cobalt, 52 stainless steel, and titanium, have been recently tested as anodes.³⁻⁸ Among these 53 54 metals, copper and stainless steel are considered as the most promising anode materials as they are relative cheap, scalable, and producing comparable current 55 density to that of graphite electrode.^{4,8} However, the relative low corrosion resistance 56 of copper and stainless steel means that they cannot be used in an uncontrolled 57 58 wastewater treatment environment (e.g. high concentration of ammonia nitrogen, salinity, oxidant and hydrogen ions) but, rather, have to be used in a well-controlled 59 environment (e.g. more reducing environment).⁹ Therefore, it is still of great 60 importance to find stable and cost-effective metal-based electrodes for MFCs. 61

Titanium has been widely used as a dimensionally stable anode in the electrolysis industry because of its excellent corrosion resistance, mechanical properties, and electric conductivity.^{10,11} However, in previous studies, the performance of titanium as 65 anode of MFCs was so poor that it was mainly used as current collectors for carbon 66 electrodes. The prior poor performance of titanium anodes in MFCs is likely because the passive layer on titanium makes them unfavorable for EAM biofilm formation and 67 inhibits electron transfer between microorganisms and the electrode.^{4, 12} Hence, 68 surface modification of titanium with biocompatible materials might be an effective 69 70 way to convert it into a high-performance anode for MFCs. TiO₂ nanoparticles are biocompatible and stable, and recently have been used to modify carbon electrode to 71 improve the power output of MFCs.^{13,14} Moreover, it has been reported that TiO₂ 72 nanotube can be in-situ synthesized used as an adhesion support platform for bone 73 and stem cells.¹³ Therefore, the aim of this study was to synthesize TiO₂ nanotube 74 arrays on a titanium plate surface and to test the performance of the modified titanium 75 electrode as a bio-anode in MFCs. 76

77

78 MATERIALS AND METHODS

79 **Preparation of TiO₂ nanotube arrays**

80 A Ti plate (purity, 99.6%, Guangzhou China; thickness 0.5 mm) was cut into 1.0 cm \times 81 2.0 cm pieces. Before modification, the Ti plates were sequentially cleaned in acetone, 82 ethanol and deionized (DI) water by ultrasonication for 30 min. The TiO_2 nanotube arrays were synthesized on the cleaned Ti plates by anodic oxidation in 5 wt. % NaF 83 electrolyte (ethylene glycol/ $H_2O = 8:2$) following the method described in an earlier 84 report.¹³ The procedure of the treatment was summarized in Fig. S1. Briefly, the Ti 85 plate was electrochemically oxidized in 5 wt. % NaF electrolyte (ethylene glycol/H₂O 86 = 8.2) in a two-electrode setup with another Ti plate (two times bigger than the anode) 87 88 as the counter electrode. The voltage was held at 30 V for 6 h and the temperature of the electrolyte was maintained at 55 °C. After that, the modified Ti plates were 89 ultrasonically cleaned in deionized (DI) water for 30 s. Finally, the Ti plates were 90 91 annealed in a muffle furnace at 450 °C for 2 h to obtain an anatase structure.

92 Characterization of TiO₂ nanotube arrays

93 The surface morphology of the anode was characterized using a field emission 94 scanning electron microscope (FESEM; SU-70, Hitachi, Japan). The surface chemical 95 composition was measured using X-ray photoelectron spectroscopy (XPS), which was 96 collected using an EscaLab 250Xi spectrometer with a monochromated Al Ka source 97 (Thermo, England). Spectra were calibrated on the Ti and O element and analyzed 98 using XPSPEAK41 software. The static water contact angles of the hybrid 99 membranes were determined by using a contact angle goniometer (DSA100, Krüss, 100 Germany).

101 Electrochemical characterization of TiO₂ nanotube arrays

All electrochemical measurements were performed using an electrochemical workstation (Biologic VSP, Claix, France) in a three-electrode cell. All potentials in this work are quoted relative to the Ag/AgCl (3.5 M KCl) reference electrode. The EIS measurements were performed at an open circuit potential, amplitude of 10 mV, and a frequency range of 100 kHz to 1 Hz in sterile M9 solution. The corrosion potential was recorded by linear sweep voltammetry (LSV) in sterile M9 solution. The potential window was -0.8 to 0.2 V and the scan rate was 0.1 mV s⁻¹.

109 **Reactor construction**

110 All electrodes were tested in a cylindrical and dual-chamber reactor, as shown in 111 detail in Fig. S2A. This reactor contained eight anodes with one cathode. The volume 112 of the anodic chamber was 800 mL and that of the cathodic chamber was 100 mL. For 113 TiO₂ nanotube arrays modification, we used four parallel electrodes that were placed 114 on opposite sides of the reactor. For other modifications, we used two parallel 115 electrodes. The compartments were separated by a cation exchange membrane 116 (CMI-7000, Membranes International, USA), which was immersed in 5% NaCl 117 solution for 24 h before use. All reactors were cultivated at a stable ambient 118 temperature (40±2 °C) controlled by a thermotank. The anolyte consisted of CH₃COONa (1 g/L), M9 solution (NH₄Cl, 0.1 g/L; NaCl, 0.5 g/L; KH₂PO₄, 4.4 g/L; 119 K₂HPO₄, 3.4 g/L; MgSO₄, 0.1 g/L; NaHCO₃, 2 g/L) and trace elements.^[20] The 120 121 anolyte was inoculated with 100 mL fresh anodic effluent (OD600 was about 1) of an 122 existing acetate-fed MFC reactor in the lab that had been continuously running for two years. The catholyte was 20 g/L K_3 [Fe(CN)₆]. The external resistance was 1 Ω (Fig. S2B) and the current generation data were collected using a data acquisition instrument (34970A, Agilent, USA). All average current densities were calculated based on the data from day 4-8.

127 Characterization of the biofilm

Current data were collected using a data acquisition instrument (34970A, Agilent, 128 USA). Biofilm CV was performed within -0.8 to 0.2 V at a scan rate of 1 mV s⁻¹ in 129 130 fresh anolyte. EIS was measured at an open circuit potential. The frequency ranged 131 from 1 kHz to 1 mHz and the polarization potential was 10 mV in fresh anolyte. After 132 acclimation for 20 days, the biofilm samples of two pieces were subjected to the 133 LIVE/DEAD BacLight bacterial viability test (LIVE/DEAD® BacLight[™] Bacterial 134 Viability Kit, Molecular Probes, USA) and captured using a fluorescence microscope 135 (DM2500, Leica, Germany). The biofilm samples of another two pieces were 136 subjected to cell disruption and then used to measure the protein concentration using the Folin's phenol reagent methods.¹⁵ 137

138 **RESULTS AND DISCUSSION**

139 Evaluation of electrode performance

140 The surface of the Ti substrate (TS) was silvery gray and shiny. After synthesis of the TiO₂ nanotube arrays (TNs), the color of surface became violet and lost its metallic 141 142 luster. SEM images (Fig. 1B-F) showed that the surface of the Ti substrate was 143 densely packed with a wave texture, whereas the TNs was neatly covered with 144 nanoscale tubes (diameter: 60–90 nm; wall thickness: ~20 nm) which resulted in an 145 increased surface area of the electrode. In addition, the Ti substrate turned blue only 146 after heat treatment at 450 °C for 2 h (HT) and its surface structure was similar to that 147 of TS, indicating that very thin titanium oxide layers were formed (Fig. S3).

High-resolution XPS scans of the Ti and O regions are shown in Fig. 1G. All of the electrodes exhibited two peaks (Ti^{4+} -1/2p and Ti^{4+} -3/2p) at binding energies of 458.7 and 465.1 eV, respectively, ^{16,17} which indicated that the surface titanium of HT and TNs was completely oxidized and formed a layer of titanium oxide. A different peak of Ti⁰ at 454.6 eV was observed on TS, which indicated that the surface titanium was oxidized in air. However, this only occurred to a limited extent on pristine titanium. In addition, the O1s XPS spectra of TNs and HT also showed a single clear peak of Ti– O=O at 531.3 eV, whereas different peaks at 530.4 (Ti–OH) and 532.8 eV (Ti–O) were observed on the surface of TS, which may be attributed to the water adsorbed on the surface.¹⁸

158 The XPS results showed that the surfaces of TNs, HT and TS had a similar 159 chemical composition. Therefore, the increase in capacitance is consistent with the increase of the BET surface area.⁶ Based on electrochemical impedance spectroscopy 160 161 (EIS) in a sterile M9 medium (Fig. S4), the surface capacitance of the TNs increased from 0.043 to 0.462 mF cm⁻², which means that the effective contact areas with the 162 water of TNs were at least 10-fold higher than that of TS. In addition, the water 163 contact angle of the TS was greater than 120° (Fig. S3B). After anodic oxidation, the 164 165 water droplet promptly integrated into the TNs electrode, indicating that the 166 hydrophobic metal surface was transformed into a hydrophilic surface in the TiO_2 167 nanotube arrays.

168 Current generation and biofilm characterization

The power output performance of TNs was tested in a cylindrical and dual-chamber reactor. Fig. 2A and S5 shows the current generation over time for the TNs, HT and TS. After 4 days of operation, the maximum projected current density ($j_{projected}$) of TNs was 12.7 ± 0.7 A m⁻² (mean ± SD, n=3), which was more than 190-fold higher than that of TS (0.07 ± 0.02 A m⁻², n=2). In addition, HT only showed a small increase in current output (0.16 ± 0.03 A m⁻², n=2), indicating the contribution of heat treatment to the enhancement of current output was very limited.

Cyclic voltammetry of the biofilm was conducted in the same medium to investigate the electrochemical activity (Fig. 2B). Compared with the electrode CVs in bare M9 medium (Fig. S6), the biofilm CVs of the TNs exhibited a classic sigmoidal shape under acetate turnover conditions, indicating that the generation of
 the current could be attributed to biofilm-associated extracellular electrons.⁶

181 Biofilms were visualized using fluorescence microscopy (Fig. 2C). The image 182 showed that the live bacteria biofilms covered 100% of the surface of the TNs, while 183 almost no biofilm was attached to the surface of TS and HT. Similarly, the protein concentration (583 \pm 55 µg cm⁻²) on TNs was approximately 15 times higher than 184 that of the TS ($38 \pm 12 \ \mu g \ cm^{-2}$) (Fig. S7). Next, we performed EIS at an open circuit 185 186 potential of the biofilm (\sim -460 mV) to measure the charge transfer process between the anode and the biofilm. As shown in Fig. 2D, the charge transfer resistance (R_{ct}) of 187 TNs was ~580 Ω , compared with ~14,800 Ω for HT and ~28,600 Ω for TS. This 188 189 improvement in resistance may be caused by the high conductive contact area between biofilm and TNs.¹⁹ In summary, these results indicated that the TiO₂ 190 191 nanotubes were suitable for biofilm formation.

192 Comparison with other high-performance anode materials

193 Prior reports of MFCs with titanium plate anodes have shown an extremely low current output (range from 0 to 0.0006 A m⁻²; see Table 1).^{4,12} The maximum current 194 195 density achieved in this study is much higher than these previous reports. It is 196 somewhat complex to compare the current densities among different researches 197 because the reactor designs, medium compositions, microbial inoculum, and 198 operational conditions are different in different research groups. However, most-commonly used graphite plate (6.0 \pm 0.6 A m⁻², n=2) and graphite felt (11.3 \pm 199 0.4 Am^{-2} , n=2) were also tested under the same conditions in this study (Fig. S8), and 200 201 the maximum current densities achieved on them were all lower than that of TNs (p< 202 (0.05), indicating that TNs was indeed a high performance anode material for MFCs.

Furthermore, the current output of TNs is also higher than that produced by other metal electrodes, such as copper, nickel, silver and gold plate electrodes. Gold and silver don't require a detailed analysis of the performance because those noble metals are cost-prohibitive in practical applications. Copper and stainless steel (SS) are commercially available on a large scale. However, these metals are susceptible to corrosion under the influence of certain ions, such as chloride from M9 solution.,⁴ When exposed to M9, the corrosion potential of these metals became more negative (copper: -0.26 V, stainless steel: -0.55 V) (Fig. S9). This propensity to corrosion would inhibit their development as bio-anodes. By comparison, titanium has the most positive corrosion potential (-0.08 V in sterile solution; -0.10 V under the presence of biofilm).

214 Additionally, table 1 also shows the comparisons of the prices of some high 215 performance materials. Titanium plate is commercially available at larger scale, and its price (30 k\$ m⁻³) is similar to graphite felt (25-75 k\$ m⁻³). The lowest material 216 costs (21 k m⁻³) is SS electrode, while since SS foam (830 – 1600 k m⁻³) and SS felt 217 $(30 - 100 \text{ k} \text{ m}^{-3})$ are not widely circulated in the market, the prices of them are much 218 219 higher than titanium. In summary, TNs has a high conductivity, corrosion-resistance, 220 and low price, improving its comparative benefit in real-world applications as a 221 bio-anode.

222

223 ASSOCIATED CONTENT

224 Supporting Information

The Supporting Information is available free of charge on the ACS Publications website.

The preparation of TiO_2 nanotube arrays (Fig. S1), schematic of the MFCs reactor setup (Fig. S2), additional SEM images (Fig. S3), and all data collected form electrode and biofilm samples (Fig. S4-S9).

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236 Notes

237 The authors declare no conflict of interest.

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Fig. 1 (A–D) Schematic illustration and SEM images for the Ti substrate after different treatments: Ti substrate (A, B), heat treatment (A, C) and Ti nanotube (A, D); (E, F) Partial enlarged detail SEM images for the Ti nanotube; (G) XPS characterization: Ti region and O region. Blue and orange lines refer to $Ti^{4+}-1/2p$ and $Ti^{4+}-3/2p$, respectively. Red and green lines refer to Ti-O=O and Ti-O, respectively.



326 Fig. 2 (A) Current output over time of MFCs with different anodes (the data of 327 graphite electrodes showed in Fig. S4). (B) Cyclic voltammetry (1 mV/s) response of 328 the anode in fresh culture. The CVs were obtained starting from the second cycle. (C) 329 Fluorescence microscopy of the biofilms on different electrodes. The biofilms were 330 stained using the LIVE/DEAD Bac-Light bacterial viability kit (live bacteria, green). 331 (D) Electrochemical impedance spectroscopy for the biotic Ti substrate after different 332 treatment at open circuit potential, an amplitude of 10 mV, and a frequency range of 1 333 kHz to 1 mHz in fresh culture.

| Metal electrodes for BESs | j projected a | Price ^b | Corrosion potential | ЪĆ |
|---------------------------------|---------------------|-------------------------|---------------------|-----|
| | (Am ⁻²) | (k\$ m ⁻³) | (V) ^c | ĸei |
| Carbon black/SS | 101 | / | / | 20 |
| SS foam | 82 | 830-1600 ^e | / | 21 |
| 254SMO SS grade | 22 | / | / | 22 |
| Flame oxidation SS felt | 19 | / | / | 6 |
| Heat-treated SS felt | 15 | 30-100 ^e | / | 7 |
| Copper electrode ^d | 15.2 | $\sim 49^{\rm f}$ | -0.26 | 4 |
| Gold electrode ^d | 11.7 | / | / | 4 |
| Silver electrode ^d | 11.1 | / | / | 4 |
| SS electrode (SUS 304) | 6.7 | $\sim 21~^{\rm f}$ | -0.55 | 4 |
| 3D macroporous on SS fiber felt | 6.1 | / | / | 23 |
| Nickel electrode ^d | 3.8 | $\sim 135\ ^{\rm f}$ | -0.21 | 4 |
| CNTs-stainless steel mesh | 3.6 | / | / | 24 |
| Surface oxygen-rich titanium | ~ 0 | / | / | 12 |
| Titanium electrode ^d | ~ 0 | / | / | 4 |
| Titanium plate (TNs) | 12.7 | $\sim 30^{\text{ g}}$ | -0.08 | * |
| Untreated graphite felt | 11.3 | \sim 25-75 $^{\rm e}$ | / | * |

335 Table 1 Summary of high-performance metal bio-anodes in MFCs

(a) Projected surface area current density; (b) Prices are given per cubic metres of electrode; (c) The corrosion potential was recorded by LSV in sterile M9 solution (Fig. S8); (d) Metal power was formed into platelike electrode by extrusion; (e) Values of stainless steel electrode substrate from Ref 25; (f) Values of those metal electrode substrate from Ref 4; (g) Values of titanium plate (approximately pure metal) form Argus metals (<u>https://www.metalprices.com/</u>)

* This study